

# **ANALYZING GUIDANCE INFORMATION USING RANDOM FORESTS FOR THERAPEUTIC IMAGE SEGMENTATION PROCESS**

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**ABSTRACT:** Labeled training data be used for challenging medical image segmentation problems to learn different characteristics of the relevant domain. The Random Forest (RF) classifiers and their learned knowledge during training and ways to exploit it for improved image segmentation. Apart early learning discriminative features, RFs also quantify their importance in classification. Feature importance is use to design a feature selection strategy critical for high segmentation and classification accuracy, and also to propose a efficiency cost in a second-order MRF framework for graph cut segmentation. The cost function combines the contribution of different image skin texture like intensity, texture, and curving information. Experimental outcome on medical images show that this strategy leads to better segmentation accuracy than conventional graph cut algorithms that use only intensity information in the smoothness cost.

**Keyword:** Medical image segmentation, Active Appearance Models, Random Forest (RF) classifiers Texture, Curvature.

## **I. INTRODUCTION**

Medical image segmentation is challenging due to image modality, organ type and segmentation framework. The task is further complicated by varying scanner parameters from different modalities, low resolution, and image noise in many cases poor contrast. Two very popular approaches for medical image segmentation are

active contour, and graph cuts. Initial works using these methods primarily relied on low level image information like intensity, texture and edge information to segment the target organ. However, image features alone were not sufficient for an accurate segmentation which fostered the exploration of ways to include prior knowledge from training datasets. Subsequently many works started incorporating prior shapes and statistical information into level sets and graph cut segmentation.

Another approach of exploiting training data is to learn image features that distinguish between organ and background structures as in Active Appearance Models (AAMs) and Active Shape Models (ASMs). In this work we propose a method that analyses the training process of Random Forest (RF) classifiers, and uses the learned knowledge to devise feature selection strategies and in segmenting medical images.

Most methods for RF based segmentation use only the probability maps to segment the desired organ. Further, while imposing smoothness constraints they use only intensity information. However, RFs can provide much more knowledge from the training procedure. RFs allow us to examine the training procedure and quantify the importance of different features to the classification task. This knowledge is useful in many ways like designing an appropriate smoothness cost, or improved feature selection that could lead to higher segmentation accuracy.

In the medical field, knowledge mainly builds upon the experience or the amount of evidences accumulated by medical experts in the hospitals all over the world. The human body is very complex machinery, that consists of many components, and which can be influenced by many factors. Hence, modeling its different functions or is a very difficult task. With its ability of generalizing from past observations and to perform predictions, machine learning seems to offer the perfect tools to integrate the experience and knowledge of medical experts into medical imaging applications.

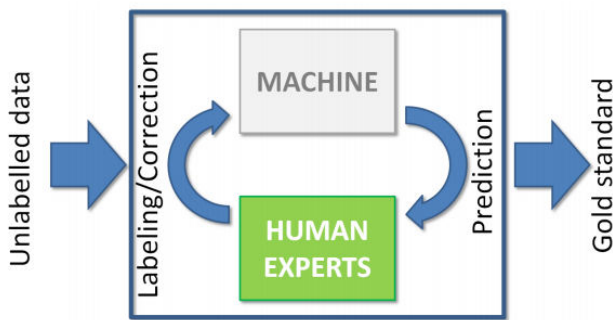


Fig 1.1: Data Predication

Since medical imaging became digital, machine learning can play a crucial role to support early diagnosis of cancer. The last decade, a lot of learning-based techniques have emerged, most of them based on a two-phases framework

- (1) Detection and/or segmentation of abnormalities,
- (2) Classification of the detected abnormality into benign or malignant.

**II. Related work**

To Shape prior segmentation method using graph cuts capable of segmenting multiple objects. The shape prior energy is based on a shape distance popular with level set approaches. We also present a multiphase graph cut framework to simultaneously segment multiple, possibly overlapping objects [3]. The multiphase formulation differs from multi way cuts in that the former can account for object overlaps by allowing a pixel to have multiple labels. We then extend the shape prior energy to encompass multiple shape priors. Unlike variation methods, a major advantage of our approach is

that the segmentation energy is minimized directly without having to compute its gradient, which can be a cumbersome task and often relies on approximations. Experiments demonstrate that our algorithm [1], The Mumford-Shah functional and its cartoon limit which facilitates the incorporation of a statistical prior on the shape of the segmenting contour. By minimizing a single energy functional, we obtain a segmentation process which maximizes both the grey value homogeneity in the separated regions and the similarity of the contour with respect to a set of training shapes [1]. We propose closed Form, parameter-resolution for incorporating invariance with respect to similarity transformations in the variation framework. We show segmentation results on artificial and real-world images with and without prior shape information. In the cases of noise, occlusion or strongly cluttered background the shape prior significantly improves segmentation [2].

**2.1.Profile Based Personalization**

Previous works on profile-based PEL mainly focus on improving the search utility. The basic idea of these works is to tailor the search results by referring to, often implicitly, a user profile that reveals an individual information goal. In the remainder of this section, we review the previous solutions to PEL on two aspects, namely the representation of profiles, and the measure of the effectiveness of personalization.

Many profile representations are available in the literature to facilitate different personalization strategies. Earlier techniques utilize term lists/vectors or bag of words to represent their profile. However, most recent works build profiles in hierarchical structures due to their stronger descriptive ability, better scalability, and higher access efficiency.

**2.1.Variation Integration of Shape Statistics and Segmentation**

The combine image information and previously acquired shape information in one variation framework. For a given contour C we define energy. The functional  $E_i$  measures how well the contour and the associated

segmentation u approximate the input grey value information. Ec favors contours which are familiar from a learning process. The parameter  $\alpha$  allows to define the relative weight of the prior. In the propose for  $E_i$  a modification of the Mumford-Shah functional and its cartoon limit, which facilitates a parameterization of the contour as a closed spine curve. Shape learning and shape statistics are then conveniently defined on the distribution of spline control points.

### 2.2. Interactive Graph Cut Based Segmentation with Shape Priors

Interactive or semi-automatic segmentation is a useful alternative to pure automatic segmentation in many applications. While automatic segmentation can be very challenging, a small amount of user input can often resolve ambiguous decisions on the part of the algorithm. In this work, we devise a graph cut algorithm for interactive segmentation which incorporates shape priors. While traditional graph cut approaches to interactive segmentation are often quite successful, they may fail in cases where there are diffuse edges or multiple similar objects in close proximity to one another. Incorporation of shape priors within this framework mitigates these problems.

### III. PREVIOUS IMPLEMENTATIONS

Random Forests are an ensemble learning method (also thought of as a form of nearest neighbor predictor) for classification and regression that construct a number of decision trees at training time and outputting the class that is the mode of the classes output by individual trees (Random Forests is a trademark of Leo Bremen and Adele Cutler for an ensemble of decision trees). Random Forests are a combination of tree predictors where each tree depends on the values of a random vector sampled independently with the same distribution for all trees in the forest. The basic principle

is that a group of “weak learners” can come together to form a “strong learner”. Random Forests are a wonderful tool for making predictions considering they do not over fit because of the law of large numbers. Introducing the right kind of randomness makes them accurate classifiers and repressors.

The Random Forests algorithm was developed by Leo Bremen and Adele Cutler

1. If the number of cases in the training set is N, sample N cases at random but with replacement, from the original data. This sample will be the training set for growing the tree.
2. If there are M input variables, a number M is specified such that at each node, m variable are selected at random out of the M and the best split on these m is used to split the node. The value of m is held constant during the forest growing. Each tree is grown to the largest extent possible. There is no pruning.

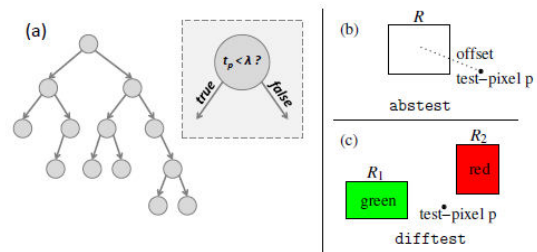


Fig 1.2 Decision Tree

### IV. SYSTEM IMPLEMENTATION

At each node  $N_l$  of the tree  $F_t$ , a splitting function  $f_l$  permits to split the subset  $S_l$  of the training set arriving in this node. As detailed in the previous section, the goal of node optimization is to find the best splitting function according to a predefined objective function. In classification tasks, several objective functions have been proposed that mostly aim at reducing the class uncertainty. In the following, we will define the most popular which the Information Gain is and a variant based on the Gain impurity. Information gain measures the difference between the class uncertainty before and

after the splitting. A common measure of uncertainty is the so-called Shannon’s entropy which is defined for discrete random variables as follows:

The random forests algorithm (for both classification and regression) is as follows:

1. Draw tree bootstrap samples from the original data.
2. For each of the bootstrap samples, grow an un pruned classification or regression tree, with the following modification: at each node, rather than choosing the best split among all predictors, randomly sample  $m$  try of the predictors and choose the best split from among those variables. (Bagging can be thought of as the special case of random forests obtained when  $m$  try =  $p$ , the number of predictors).
3. Predict new data by aggregating the predictions of the  $n$  tree trees (i.e., majority votes for classification, average for regression). An estimate of the error rate can be obtained, based on the training data, by the following:

1. At each bootstrap iteration, predict the data not in the bootstrap sample (what Breiman calls “out-of-bag”, or OOB, data) using the tree grown with the bootstrap sample.

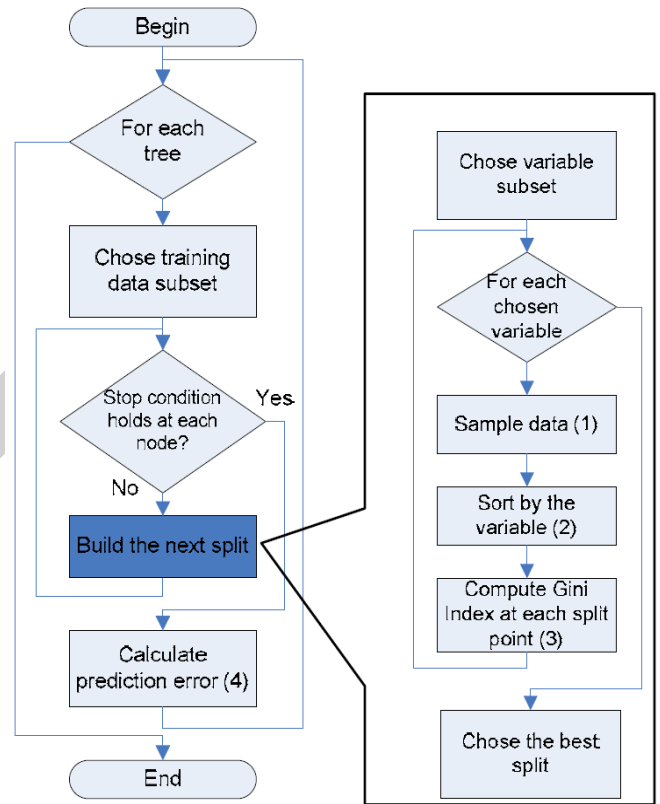


Fig 1.3: Random Forest Algorithm

2. Aggregate the OOB predictions. (On the average, each data point would be out-of-bag around 36% of the times, so aggregate these predictions.) Calculate the error rate, and call it the OOB estimate of error rate.

#### 4.1 Image Features

This section describes the features used in our method - intensity statistics, texture and curvature anisotropy, and spatial context features. Context features are a combination of intensity, texture and curvature values sampled using a template. ROI identification requires classification of super pixels for which we use intensity, texture and curvature features, (excluding context information) to ensure fast feature extraction and subsequent classification, as well as good generalization of the classifier. For generating ROI probability maps we employ the complete set of features (including context information).

#### 4.2 Intensity Statistics

It is not always easy to identify the edges of the RV blood pool and surrounding myocardium wall. Psychophysical experiments have established that the human visual system (HVS) is sensitive only to image features of the first and second order (mean and variance). However, MR images commonly contain regions that do not form distinct spatial patterns but differ in their higher order statistics, e.g. boundaries of some malignant tumors are diffuse and invisible to the naked eye. Therefore, in addition to features processed by the HVS, we propose to investigate features that are not discernible by the human eye but may provide discriminating information for our task. For every sub-region (super pixel or pixel neighborhood) we calculate the mean, variance, skewness and kurtosis of the intensity values.

#### 4.3 Texture Anisotropy

Texture is modeled as patterns distinguished by a high concentration of localized spatial frequencies. 2-D Gabor filter banks are used to generate texture maps for each image. Gabor filters have optimal joint localization in the spatial and frequency domains. Their multi-scale and multi orientation structure conforms to the receptive field profiles of simple cortical cells, and captures rich visual properties such as spatial localization, orientation selection and spatial frequency characteristics. Since Gabor filters incorporate Gaussian smoothing they are robust to noise.

$$\chi_{ani}^r = - \sum_{tex} p_{tex}^r \log p_{tex}^r \quad (1)$$

Texture maps are partitioned into 9 equal parts corresponding to 9 sectors of a circle, and the entropy of texture values is calculated for each sector. More sectors led to fewer samples per sector which jeopardizes estimation of stable higher order statistics. Too few

#### 4.4 Region of Interest Identification

ROI identification is an important part of our method because:

- 1) It reduces the total computation time since we need not classify each pixel; and
- 2) The ROI gives an initial selection of likely RV pixels and

reduces false positives in subsequent analysis. Intensity in homogeneity correction was performed using the nonparametric non uniform intensity normalization (N3) method.

$$Curv_{ani}^r = - \sum_{\theta} p_{\theta}^r \log p_{\theta}^r \quad (2)$$

Denotes the probability distribution of curvature values in sector r, 0 denotes the curvature values. Similar to texture anisotropy, the curvature asymmetry measure is also a 9 dimensional feature vector for a region.

$$x' = s_1 + \frac{x - p_1}{p_2 - p_1} (s_2 - s_1) \quad (3)$$

Where x' is the new intensity obtained from the original intensity value x; s1, s2 are the minimum and maximum intensities of the test image. This approach leads to good contrast of the different images.

#### 4.5 Algorithm Implementation

##### Algorithmic Analysis:

- Generate the initial population of individuals
- Calculate the fitness value for each individual in that population
- Repeat on this generation until stop condition is met: (time limit, sufficient fitness achieved, etc.)
- Select the best-fit individuals for reproduction
- Create new individuals by applying crossover and mutation operations
- Evaluate the individual fitness of new individuals

#### EVALUATION RESULT:

##### Probability maps and Graph Cut Segmentation

Probability maps are generated for all ROI pixels using a second set of RF classifiers. Approximately equal number of samples from RV and background pixels is taken from the training datasets. Intensity, texture, curvature and context features derived from these samples were used to train a RF classifier (different from the one trained on super-pixel features). The features were extracted from a 31 × 31 neighborhood of each pixel. The training set varies with each round of cross validation. The trained classifier is used to generate

probability maps for every pixel within the identified ROI. Each pixel has 3 probability values corresponding to the blood pool, myocardium and background. The probability maps serve as penalty costs in a second order MRF cost function.

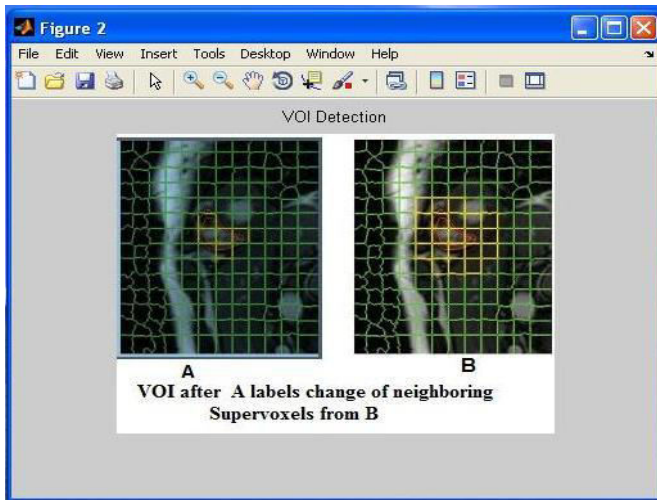


Figure 1.4: VOI Detection

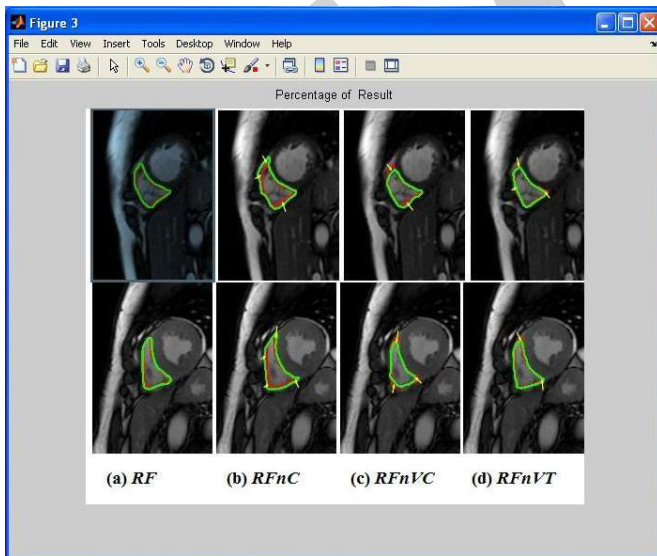


Fig 1.5:RV Segmentation results (a) RF;(b) RFnC; (c)RFnVC ; and (d) RFnVT

## EXPERIMENTS AND RESULTS

Cardiac MR Examinations were performed at 1.5T (Symphony Tim, Siemens Medical Systems, Erlangen, Germany) using a eight-element phased-array cardiac coil and repeated breath-holds of 10 – 15 s. A total of 8 – 12 contiguous cine short axis slices were performed. Sequence parameters were as follows: TR = 50 ms; TE = 1.7 ms; flip angle = 55; slice thickness = 7 mm; matrix size = 256×216; Field of view = 360–420 mm; 20 images per cardiac cycle; spatial resolution of 0.75mm/pixel. There were 32 datasets and we use a leave-one-out strategy to evaluate our method.

$\lambda$	10	5	1	0.5	0.1	0.0	0.0	0.00
						1	2	1
D	74.	74.	77.	80.	83.	84.	89.	89.7
M	2	8	2	8	7	6	6	

Table 2 Change in segmentation accuracy with different values of  $\lambda$  (Eqn. 3).

N	300-600	600-900	900-1200
Acc <sub>BP</sub> (%)	77.9±1.6	89.8±2.9	83.5±2.7
Acc <sub>Myo</sub> (%)	75.1±2.8	88.5±2.3	80.8±3.2
Acc <sub>B</sub> (%)	74.7±2.8	89.3±2.8	80.0±2.7

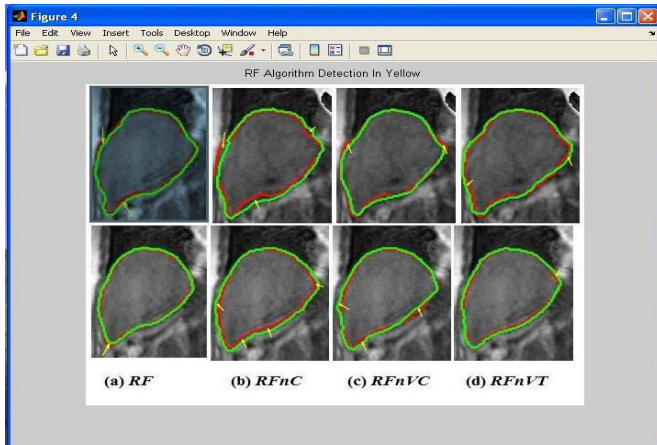


Figure 6.4 Liver Segmentation Results

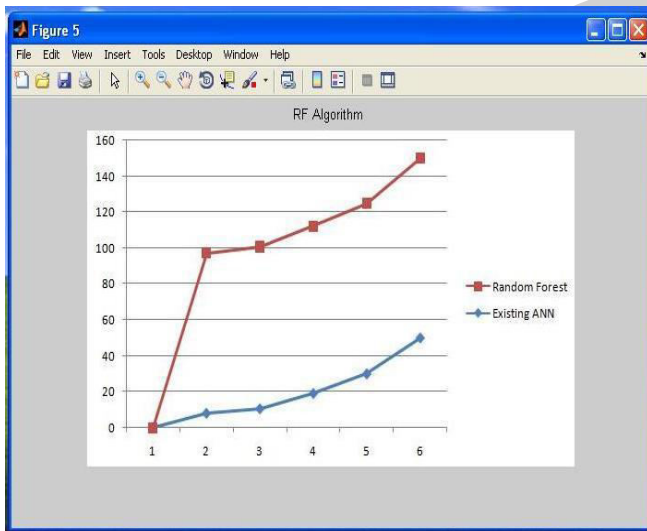


Figure 6.5 Performance of Random Forest

## CONCLUSION

We have proposed an image segmentation method that exploits knowledge from the training process of Random forest classifiers. Apart from learning discriminative features, RFs allow us to examine the role of different features and their contribution toward classification accuracy. Hence we are able to quantify the importance of different features to the classification task. These importance measures are used to design a smoothness cost for graph cut segmentation by weighing different features like intensity, texture and curvature

according to their importance in classification. This strategy allows us to segment challenging cases where the desired organ in MR images has similar appearance to its surrounding regions. It results in higher segmentation accuracy than conventional graph cut approaches that use only intensity information in the smoothness cost. Thus we are able to weight different features automatically and avoid the shortcomings of ad-hoc weighting strategies. This knowledge is particularly useful when the number of samples is low when compared with the number of feature elements. In such a case the trained RF may not generalize well to novel samples. We can choose to discard those feature elements that have minimal influence on the classification performance. In doing so we can achieve better generalization of the RF in spite of very few samples.

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